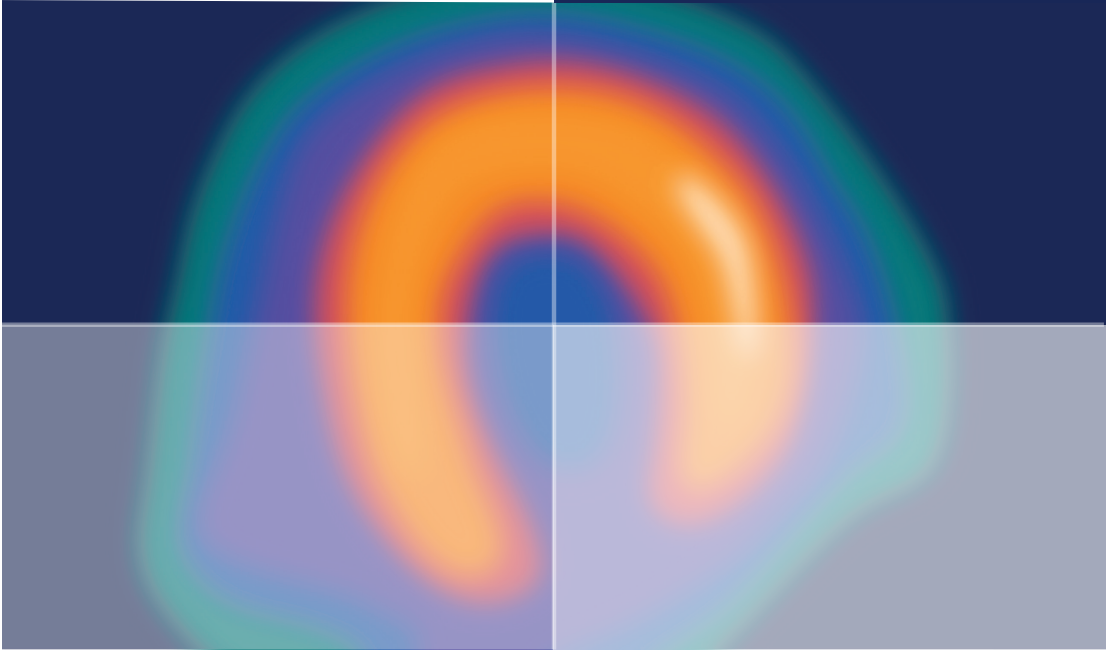




READY
for **PET**



Clinical Value of Cardiac PET

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OVERVIEW

There is growing excitement in the nuclear cardiology community regarding the emerging role of cardiac positron emission tomography (PET) myocardial perfusion imaging (MPI) for assessment of coronary artery disease (CAD) and other cardiovascular conditions. The purpose of this monograph is to highlight the clinical value of cardiac PET by outlining the many advantages it offers in managing patients with known or suspected CAD (*Table 1*).

Advantages of Cardiac PET
• Excellent diagnostic accuracy
• Consistently high image quality
• Protocol efficiency
• Low radiation exposure
• Peak-stress imaging and left ventricular ejection fraction (LVEF) reserve
• Myocardial blood flow (MBF) and myocardial blood flow reserve (MBFR)
• Coronary artery calcification assessment with PET/CT systems
• Robust prognostic data
• Applications beyond myocardial perfusion imaging

Table 1. Advantages of cardiac PET

EXCELLENT DIAGNOSTIC ACCURACY

PET MPI with myocardial blood flow reserve (MBFR) has been shown to have a higher diagnostic accuracy than other imaging modalities in a head-to-head study using invasive fractional flow reserve as the reference standard.¹ (*Figure 1*)

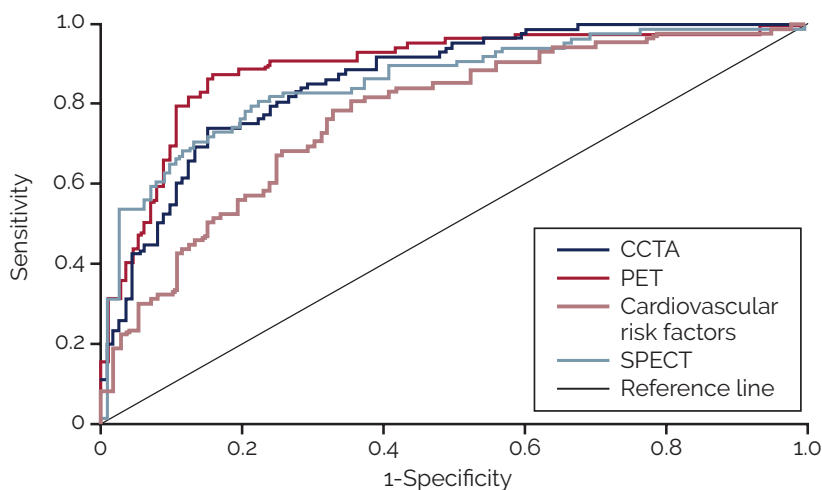


Figure 1. Diagnostic performance of cardiac imaging methods and traditional cardiovascular risk factors for the detection of coronary artery disease on a patient-based level.¹

In this study, diagnostic accuracy was highest for PET (85%) compared with SPECT (77%) and CCTA (74%). The reasons for the high clinical performance of PET are multifactorial, including superior PET tracer properties and instrumentation, robust attenuation and scatter correction, and the ability to quantify absolute MBF and MBFR. Fundamental characteristics of PET imaging are summarized in *Table 2*.

Characteristics of PET	
Attenuation correction	Routine and robust
Scatter correction	Routine and robust
Spatial resolution	Good (^{82}Rb) to excellent ($^{13}\text{N-NH}_3$, $^{18}\text{F-flurpiridaz}$)
Myocardial tracer uptake	Moderate (^{82}Rb) to high ($^{13}\text{N-NH}_3$, $^{18}\text{F-flurpiridaz}$)
Timing of stress imaging	Peak-stress (^{82}Rb) or early post-stress ($^{13}\text{N-NH}_3$)

Table 2. Characteristics PET

Figure 2 illustrates the excellent image quality obtained with both ^{82}Rb and $^{13}\text{N-NH}_3$ MPI. Note the good separation of tracer uptake in the liver from the myocardium.

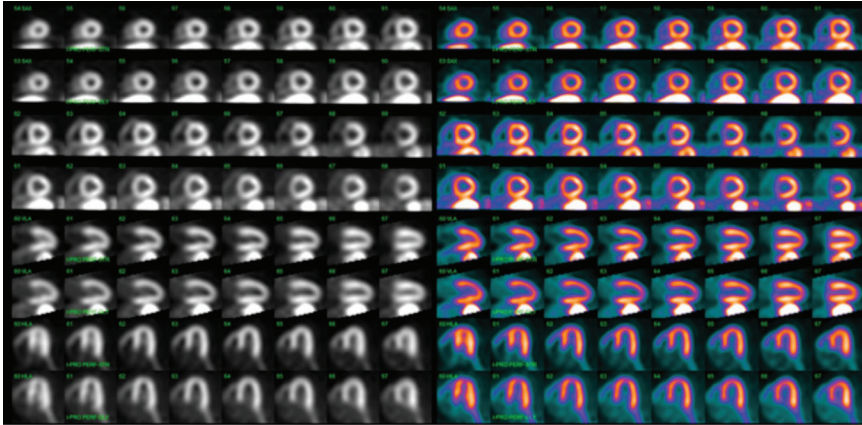


Figure 2a. Normal ^{82}Rb MPI study (Image courtesy of Timothy Bateman, MD)

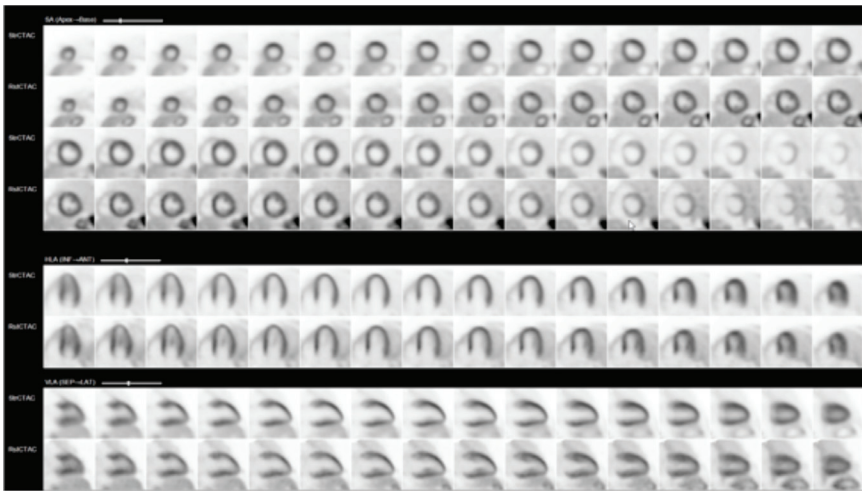


Figure 2b. Normal $^{13}\text{N-NH}_3$ MPI study (Image courtesy of Marcelo Di Carli, MD)

Attenuation correction (AC) is used routinely for PET MPI. Routine and robust attenuation and scatter correction results in an accurate reflection of the myocardial tracer activity, with images less impacted by the patient's body size or shape.

PET systems also have high spatial resolution, 2.5 to 6.0 mm. The high spatial resolution allows for the detection of small areas of hypoperfusion and is one of the reasons for the high sensitivity of PET MPI. In addition, this high spatial resolution helps to mitigate any contamination of the left ventricle from adjacent splanchnic activity. PET spatial resolution is higher for $^{13}\text{N-NH}_3$ and ^{18}F -flurpiridaz compared to ^{82}Rb due to differences in positron energy and resulting positron range, though high-quality diagnostic images are consistently obtained with all 3 radionuclides.

PET perfusion tracers demonstrate superior myocardial uptake leading to an accurate assessment of the true extent and severity of ischemia (*Figure 3*).² This in turn allows detection of flow heterogeneity and perfusion defects in the distribution of less-severe (but flow-limiting) coronary artery stenoses, improving the ability to identify the presence of multivessel CAD accurately.³

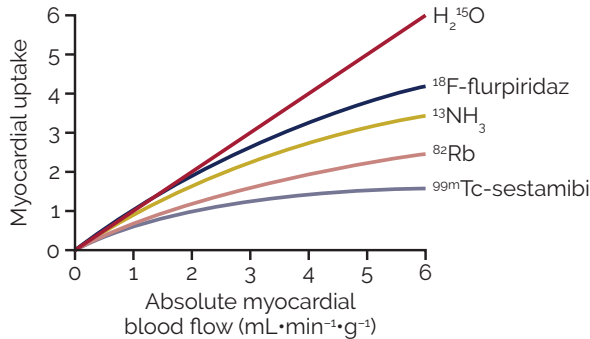


Figure 3. Kinetics of MPI perfusion tracers. Graphical representation of the relationship between absolute MBF and actual tracer uptake. Note that the PET MPI tracers demonstrate favorable myocardial uptake versus flow leading to high sensitivity for detection of multivessel coronary artery disease.²

Typically, there are trade-offs required in selecting an imaging modality for assessment of CAD, as selecting a test with high sensitivity usually requires sacrificing specificity; however, selecting PET MPI for assessment of CAD results in both high sensitivity and high specificity, and no clinical trade-off is required.

PROTOCOL EFFICIENCY

A complete rest-stress ⁸²Rb PET MPI study can be performed in as little as 20 to 35 minutes, greatly enhancing patient convenience and comfort as well as laboratory efficiency. ¹³N-NH₃ rest-and-stress studies typically can be completed in 25 to 60 minutes, depending on the protocol utilized. The rapid-imaging protocols for PET MPI allow for late afternoon scheduling resulting in reduced hospital length of stay. The excellent efficiency of PET MPI was particularly beneficial during the height of the COVID-19 pandemic when minimizing the time of close contact between patients and staff was critically important.

LOW RADIATION DOSIMETRY

Radiation exposure for PET MPI is very low, with effective doses in the range of 1 to 3 mSv for ⁸²Rb and 2 to 4 mSv for ¹³N-NH₃.⁴⁻⁸ Furthermore, because of the short half-lives of ⁸²Rb (76 seconds) and ¹³N-NH₃ (10-minutes), there is low radiation exposure to hospital personnel and family members, as the PET tracer decay is nearly complete before the patient leaves the PET imaging suite. The low radiation dosimetry of PET MPI is especially advantageous for serial imaging of patients with complex chronic CAD to limit the cumulative lifetime radiation exposure and for imaging younger patients. PET MPI allows nuclear cardiology laboratories to achieve easily the desired less than 9 mSv average

radiation dose recommended by the American Society of Nuclear Cardiology (ASNC). For purposes of reducing radiation dose, ASNC recommends using PET MPI as the first-line test when it is available.⁹

PEAK-STRESS IMAGING AND LEFT VENTRICULAR EJECTION FRACTION (LVEF) RESERVE

The timing of stress image acquisition is another important feature of PET MPI. Stress images with PET MPI are acquired at peak-stress (with ^{82}Rb) or early post-stress (with $^{13}\text{N-NH}_3$). Therefore, the change in the left ventricular ejection fraction (LVEF) between rest and stress provides powerful diagnostic and prognostic information. When using $^{13}\text{N-NH}_3$, gated PET images are acquired over 10 to 15 minutes, beginning 1.5 to 3 minutes after completion of the infusion of the pharmacologic stressor and therefore represents a blend of “peak-stress” and “early post-stress” images.¹⁰ Gated PET images, using ^{82}Rb , are acquired over 5 to 7 minutes, beginning within 1 to 2 minutes after pharmacologic stress agent infusion and therefore represent true “peak-stress” images. LVEF and left ventricular volumes can be compared on resting and peak-stress gated ^{82}Rb PET images. In normal subjects, LVEF increases and left ventricular end-systolic volume (LVESV) declines on peak-stress gated ^{82}Rb PET images compared to resting images. A normal “LVEF reserve” (defined as peak-stress LVEF minus resting LVEF) of greater than or equal to 5% has a 97% negative predictive value for excluding left main or 3-vessel CAD.¹¹ In patients with severe and extensive obstructive CAD, the LVEF declines at peak-stress (LVEF reserve is negative) and LVESV increases at peak-stress, providing additional markers of high-risk CAD beyond perfusion findings.

MYOCARDIAL BLOOD FLOW QUANTIFICATION

Perhaps the single greatest advantage of PET MPI is its ability to quantify MBF in absolute units at rest and during peak hyperemic stress. This allows calculation of the MBFR, defined as the ratio of stress to resting MBF. Global MBFR has been demonstrated to have diagnostic value,¹¹ prognostic value,¹² and can be used to guide decisions regarding likelihood of benefit from early myocardial revascularization.¹² Quantification of MBFR can also be used to identify coronary microvascular disease and to verify appropriate response to the pharmacologic stress agent.¹³ The tremendous clinical value of MBF quantification with PET MPI will be covered in detail in a separate monograph in this series.

CORONARY ARTERY CALCIFICATION ASSESSMENT WITH PET/CT SYSTEMS

The low-dose non-contrast CT images acquired for attenuation correction of PET/CT MPI studies can be used to assess for the presence of coronary artery calcification (CAC) as a marker of the presence of coronary artery atherosclerosis.¹⁴ Alternatively, a formal coronary artery calcium score can be acquired to quantify CAC as part of the routine PET/CT protocol for patients without a prior history of documented CAD. In a patient with a normal PET MPI study, the absence of detectable CAC implies an excellent long-term prognosis. Conversely, the finding of CAC in a patient with an otherwise normal PET MPI study indicates the presence of subclinical nonobstructive coronary atherosclerosis and is associated with a higher rate of cardiac events and death in proportion to the amount of CAC. These patients will benefit from more aggressive risk-factor modification and closer clinical follow-up.

Assessment of CAC can also be helpful in guiding management for patients with normal “relative” PET perfusion images but with reduced global MBFR. In this scenario, absence of CAC makes balanced myocardial ischemia due to multivessel CAD very unlikely and suggests the presence of coronary microvascular disease or a failure to respond to vasodilator stress. Conversely, the presence of severe CAC indicates extensive coronary atherosclerosis and therefore increases the likelihood of balanced myocardial ischemia. Depending on the severity of the reduction in the MBFR and the LVEF reserve, further testing (possibly including invasive coronary angiography) may be indicated. *Table 3* summarizes the clinical information provided by PET/CT.

Clinical information available from PET/CT	
Perfusion relative to the most normal region	Yes
Resting and peak-stress (or early post-stress) LVEF and wall motion	Yes
Resting and peak-stress MBF and MBFR	Yes
LVEF reserve	Yes
Verification of response to vasodilator stress	Yes
Coronary artery calcification	Yes
LVEF, left ventricular ejection fraction; MBF, myocardial blood flow; MBFR, myocardial blood flow reserve	

Table 3. Clinical information available from PET/CT

APPLICATIONS BEYOND MYOCARDIAL PERFUSION IMAGING

The combination of perfusion and myocardial metabolism using ¹⁸F-fluorodeoxyglucose (¹⁸F-FDG) remains the gold standard for clinical assessment of myocardial viability and is the only imaging modality capable of directly identifying the presence and extent of hibernating myocardium.¹⁵ ¹⁸F-FDG is also clinically useful for the assessment of cardiac sarcoidosis with several advantages compared to cardiac MRI (CMR) for sarcoidosis assessment (*Table 4*).¹⁶

¹⁸ F-FDG PET versus CMR for cardiac sarcoidosis		
	¹⁸ F-FDG PET	CMR
Detection of fibrosis / scar	++	+++
Measurement of LVEF and wall motion	+++	+++
Able to distinguish scar from active inflammation	+++	+
Assess response to therapy	+++	+
Feasible with severe renal failure	+++	+
Feasible with all CIEDs	+++	–

CIED, cardiac implantable electronic device; CMR, cardiac MRI; LVEF, left ventricular ejection fraction.

Table 4. ¹⁸F-FDG PET versus CMR for cardiac sarcoidosis

¹⁸F-FDG is also useful for the assessment of infective endocarditis and cardiac implantable electronic device (CIED) infection.^{17–20} It can be used not only to assess for the presence and extent of the cardiac infection but can also be useful in the assessment of extra-cardiac complications, such as septic emboli. ¹⁸F-FDG also plays an important role in the evaluation of vasculitis and vascular graft infections. Lastly, several PET agents are being investigated for cardiac amyloid imaging, including ¹⁸F-florbetapir, ¹⁸F-florbetaben, ¹⁸F-flutemetamol,²¹ and ¹⁸F-sodium fluoride.²²

THE CLINICAL VALUE OF CARDIAC PET

The clinical value of a cardiac imaging test can be defined both by its quality and cost-effectiveness. Quality can be thought of as directly proportional to the clinical information provided by the imaging test and inversely proportional to the radiation exposure. Using this definition, PET MPI clearly demonstrates superior quality as there is abundant clinical information provided (*Table 3*) at a low radiation dose. Similarly, the cost effectiveness of a cardiac imaging study can be defined as being directly proportional to the quality of the study and inversely proportional to its cost, both direct and indirect. PET MPI has the potential to reduce overall healthcare costs by facilitating earlier hospital discharge and reducing the need for layered testing and unnecessary invasive coronary angiography.²³

CONCLUSION

Cardiac PET has emerged as a powerful tool for evaluation of patients with coronary artery disease and other cardiac conditions. The use of cardiac PET is expected to grow with increased availability of PET cameras, enhanced software programs, and new PET perfusion tracers (e.g., ¹⁸F-flurpiridaz). The ability of cardiac PET to measure MBF and MBFR provides a powerful tool for the clinical evaluation of patients with CAD and other cardiac conditions.

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REFERENCES

1. Danad I, Raijmakers PG, Driessen RS, Leipsic J, Raju R, Naoum C, et al. Comparison of coronary CT angiography, SPECT, PET, and hybrid imaging for diagnosis of ischemic heart disease determined by fractional flow reserve. *JAMA Cardiol.* 2017; 2:1100-1107.
2. Danad I, Raijmakers PG, Knaapen P. Diagnosing coronary artery disease with hybrid PET/CT: It takes two to tango. *J Nucl Cardiol.* 2013;20:874-890.
3. Parker MW, Iskandar A, Limone B, Perugini A, Kim H, Jones C, et al. Diagnostic accuracy of cardiac positron emission tomography versus single photon emission computed tomography for coronary artery disease. A bivariate meta-analysis. *Circ Cardiovasc Imaging.* 2012;5:700-707.
4. Cerqueira MD, Allman KC, Ficaro EP, Hansen CL, Nichols KJ, Thompson RC, et al. Recommendations for reducing radiation exposure in myocardial perfusion imaging. *J Nucl Cardiol.* 2010;17:709-718.
5. Hunter CR, Hill J, Ziadi MC, Beanlands RSB, deKemp RA. Biodistribution and radiation dosimetry of ⁸²Rb at rest and during peak pharmacologic stress in patients referred for myocardial perfusion imaging. *Eur J Nucl Med Mol Imaging.* 2015;42(7):1032-1042.
6. Dorbala S, Di Carli MF, Delbeke D, Abbara S, DePuey EG, Dilsizian V, et al. SNMMI/ASNC/SCCT guideline for cardiac SPECT/CT and PET/CT 1.0. *J Nucl Med.* 2013;54(8):1485-1507.
7. Case JA, deKemp RA, Slomka PJ, Smith MF, Heller GV, Cerqueira MD. Status of cardiovascular PET radiation exposure and strategies for reduction: An Information Statement from the Cardiovascular PET Task Force. *J Nucl Cardiol.* 2017;24:1427-1439.
8. Desiderio MC, Lundbye JB, Baker WL, Farrell MB, Jerome SD, Heller GV. Current status of patient radiation exposure of cardiac positron emission tomography and single-photon emission computed tomographic myocardial perfusion imaging. A report from the Intersocietal Accreditation Commission Database. *Circ Cardiovasc Imaging.* 2018;11(12):e007565.
9. Bateman TM, Dilsizian V, Beanlands RS, DePuey EG, Heller GV, Wolinsky DA. American Society of Nuclear Cardiology and Society of Nuclear Medicine and Molecular Imaging Joint Position Statement on the Clinical Indications for Myocardial Perfusion PET. *J Nucl Cardiol.* 2016;23:1227-1231.

10. Dilsizian V, Bacharach SL, Beanlands RS, Bergmann SR, Delbeke D, Gropler RJ, et al. PET myocardial perfusion and metabolism clinical imaging. *J Nucl Cardiol.* 2009;16:651.
11. Dorbala S, Vangala D, Sampson U, Limaye A, Kwong R, Di Carli MF. Value of vasodilator left ventricular ejection fraction reserve in evaluating the magnitude of myocardium at risk and the extent of angiographic coronary artery disease: a 82Rb PET/CT study. *J Nucl Med.* 2007;48:349-358.
11. Naya M, Murthy VL, Taqueti VR, Foster CR, Klein J, Garber M, et al. Preserved coronary flow reserve effectively excludes high-risk coronary artery disease on angiography. *J Nucl Med.* 2014;55(2):248-255.
12. Patel KK, Spertus JA, Chan PS, Sperry BW, Badarin FA, Kennedy KF, et al. Myocardial blood flow reserve assessed by positron emission tomography myocardial perfusion imaging identifies patients with a survival benefit from early revascularization. *Eur Heart J.* 2020;41(6):759-768.
13. Schindler TH, Dilsizian V. Coronary microvascular dysfunction. Clinical considerations and noninvasive diagnosis. *JACC Cardiovasc Imaging.* 2020;13(1 Pt 1):140-155.
14. Einstein AJ, Johnson LL, Bokhari S, Son J, Thompson RC, Bateman TM, et al. Agreement of visual estimation of coronary artery calcium from low-dose CT attenuation correction scans in hybrid PET/CT and SPECT/CT with standard Agatston score. *J Am Coll Cardiol.* 2010;56(23):1914-1921.
15. Abraham A, Nichol G, Williams KA, Guo A, deKemp RA, Garrard L, et al. 18F-FDG PET imaging of myocardial viability in an experienced center with access to 18F-FDG and integration with clinical management teams: the Ottawa-FIVE substudy of the PARR 2 trial. *J Nucl Med.* 2010;51(4):567-574.
16. Chareonthaitawee P, Beanlands RS, Chen W, Dorbala S, Miller EJ, Murthy VL, et al. Joint SNMMI-ASNC expert consensus document on the role of 18F-FDG PET/CT in cardiac sarcoid detection and therapy monitoring. *J Nucl Cardiol.* 2017;58(8):1341-1353.
17. Chen W, Kim J, Molchanova-Cook OP, Dilsizian V. The potential of FDG PET/CT for early diagnosis of cardiac device and prosthetic valve infection before morphologic damages ensue. *Curr Cardiol Rep.* 2014;16(3):459-466.
18. Mahmood M, Kendi AT, Ajmal S, Farid S, O'Horo JC, Chareonthaitawee P, et al. Meta-analysis of 18F-FDG PET/CT in the diagnosis of infective endocarditis. *J Nucl Cardiol.* 2019;26:922-935.
19. Juneau D, Golfam M, Hazra S, Erthal F, Zuckier LS, Bernick J, et al. Molecular Imaging for the diagnosis of infective endocarditis: A systematic literature review. *Int J Cardiol.* 2018;253:183-188.

20. Juneau D, Mohammad Golfam M, Hazra S, Zuckier LS, Garas S, Calum Redpath C, et al. Positron emission tomography and single-photon emission Computed tomography imaging in the diagnosis of cardiac implantable electronic device infection: A systematic review and meta-analysis. *Circ Cardiovasc Imaging*. *Circ Cardiovasc Imaging*. 2017;10(4):e005772. doi: 10.1161/CIRCIMAGING.116.005772
21. Gallegos C, Miller EJ. Advances in PET-based cardiac amyloid radiotracers. *Curr Cardiol Rep*. 2020;22(6):40. doi: 10.1007/s11886-020-01284-3.
22. Morgenstern R, Yeh R, Castano A, Maurer MS, Bokhari S. 18Fluorine sodium fluoride positron emission tomography, a potential biomarker of transthyretin cardiac amyloidosis. *J Nucl Cardiol*. 2018;25:1559-1567.
23. Merhige M, Breen WJ, Shelton V, Houston T, D'Arcy BJ, Perna AF. Impact of myocardial perfusion imaging with PET and (82)Rb on downstream invasive procedure utilization, costs, and outcomes in coronary disease management. *J Nucl Med*. 2007;48(7):1069-1076.

NOTES



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